

Analysis of pressure drop in blood vessels with a barrier of moving blood clots using the Lattice-Boltzmann Method.

- J. Manuel Sausedo Solorio (A.A.I.A)
- M. TERESA MÉNDEZ BAUTISTA (A.A.C.T.M.)

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- It is analyzed a small thrombus just after the moment it breaks up
- Numerical calculations are performed with a computer model of a flow through a pipe with an obstacle therein.
- Temporal behavior of pressure drop and velocity of blood through moving clots is studied.

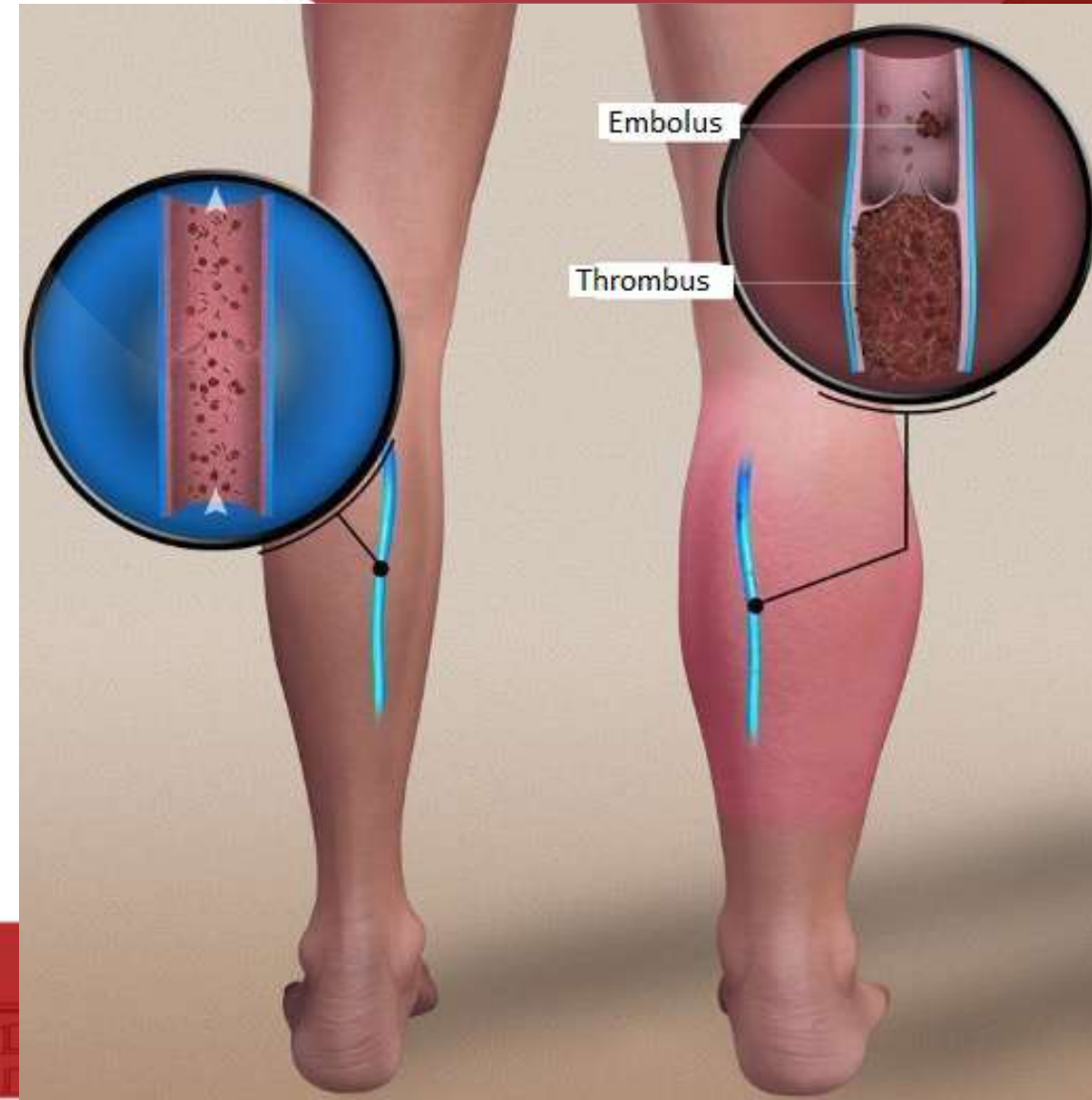
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- Relationships between the variation of the obstacle effective area and the pressure drop is found.
- The pressure variation measured before and after the moving obstacles region only depends on the temporal change of the effective dry area of obstacle.



- Thrombosis is the formation of a blood clot in a blood vessel.
- Figure shows a vein in its normal state as well as one having a thrombus.
- The clot can break loose and travel to another place in veins.



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Navier-Stokes Equations

Continuity Equation

$$\nabla \cdot \vec{V} = 0$$

Momentum Equations

$$\rho \frac{D\vec{V}}{Dt} = -\nabla p + \rho \vec{g} + \mu \nabla^2 \vec{V}$$

Total derivative

Pressure gradient

Body force term

Diffusion

$$\rho \left[\frac{\partial \vec{V}}{\partial t} + (\vec{V} \cdot \nabla) \vec{V} \right]$$

Fluid flows in the direction of largest change in pressure.

External forces, that act on the fluid (gravitational force)

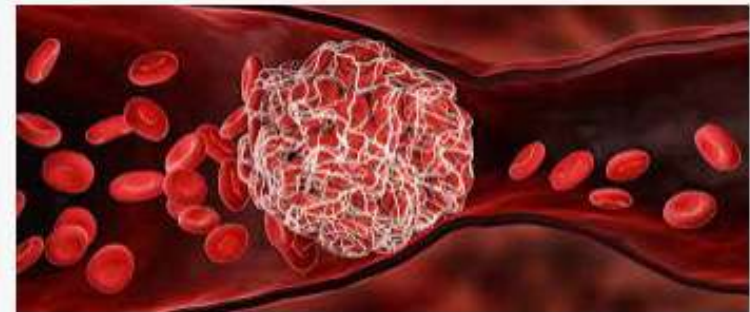
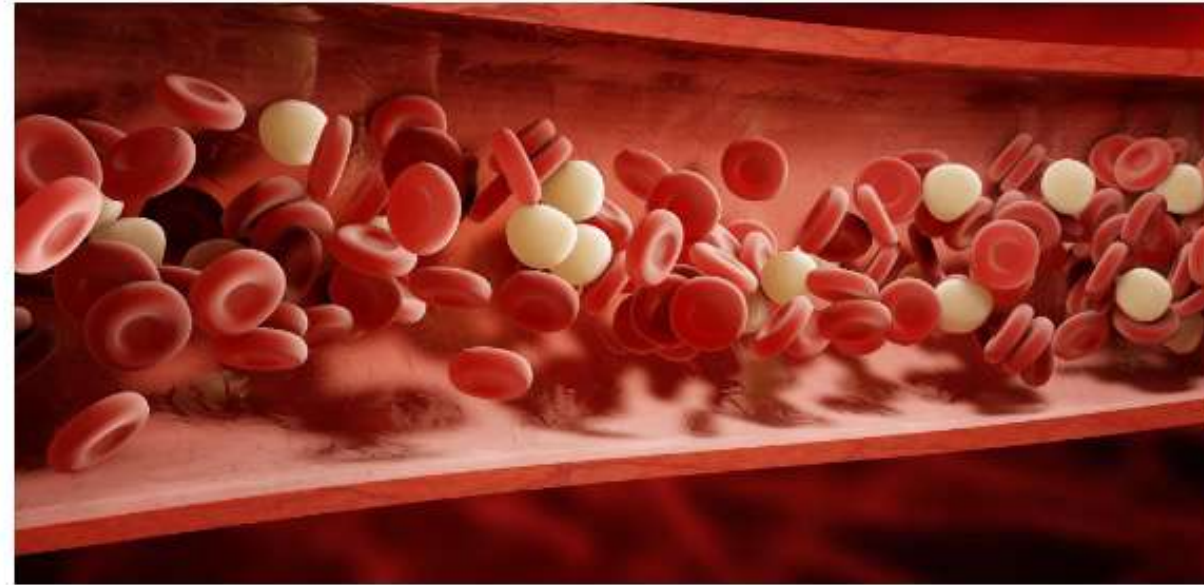
For a Newtonian fluid, viscosity operates as a

2 - Momentum Energy:

- Few analytical solutions for real fluids (i.e. Navier-Stokes equations).
- Instead, numerical solution techniques are used: solve such equations using **the Lattice-Boltzmann Method (LBM)**.

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- The temporal evolution is studied using the Lattice-Boltzmann method.
- The moving particles have autonomous random motion, producing time-varying intermittent thin streams through which the blood travels.



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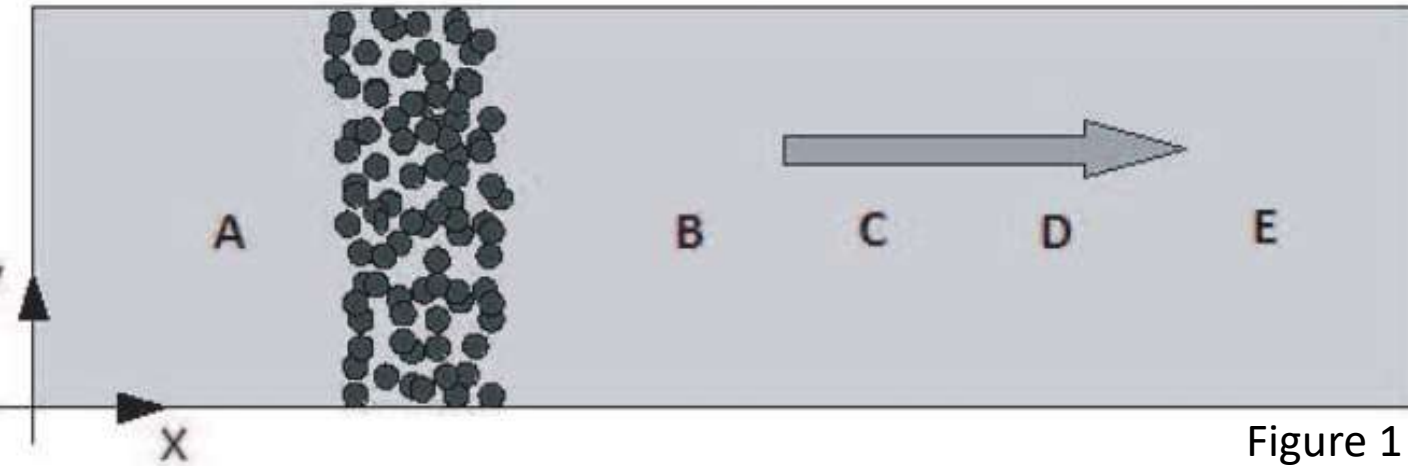


Figure 1

- ▶ Two-dimensional model. The strip obstacle is made up of small grains, so the effective area varies in time. Points with labels A, B, C, D and E are locations to get samples of variables.

- The LBM is especially useful for modeling **complicated** interfaces and **boundary conditions**, as well as **moving frontiers**.



- The scale of analysis is the size of clots, about 5% of a typical vein diameter.
- Clots displacements are assumed to obey a Uniform Probability Distribution Function (2D).
- System is modeled with a two-dimensional long tube with rectangular geometry of size $L_y = 400$ nodes high, and $L_x = 3000$ nodes wide; both dimensions in lattice units [a.u.].

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- The Boltzmann equation is described in terms of the probability distribution function f of the particles at the time t located at position x with velocity ξ defined by

$$\frac{\partial f}{\partial t} + \xi \cdot \frac{\partial f}{\partial x} + \mathbf{F} \cdot \frac{\partial f}{\partial \xi} = \Omega(f) \quad (1)$$

where $\Omega(f)$ is the collision operator which models the interaction between particles.



- For an average time τ between a pair of particle-collisions, the collision term $\Omega(f)$ is defined by $\Omega(f) = -(f - f^{eq})/\tau$, and the function f^{eq} is

$$f^{eq} = \frac{\rho}{(2\pi c_s^2)^{\frac{d}{2}}} e^{-\frac{(\xi - \mathbf{u})^2}{2c_s^2}} \quad (2)$$

where $\mathbf{u}$ is the average velocity of the particles, c_s the speed of sound, and $d=2$ (two-dimensional space).

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- A Taylor-expansion of the function f^{eq} leads to:

$$f_i^{eq} = \rho w_d \left\{ 1 + 3 \frac{\hat{e}_i \cdot \mathbf{v}}{c^2} + \frac{9}{2} \frac{(\hat{e}_i \cdot \mathbf{v})^2}{c^4} - \frac{9}{2} \frac{v^2}{c^2} \right\} \quad (3)$$

where w_d are weight factors for each direction. Direction $\hat{e}_i$ and corresponding value of w_i are {0} 4/9; {1, 2, 3, 4} 1/9; {5, 6, 7, 8} 1/36.

- This model is referred as the **D2Q9 Lattice**.

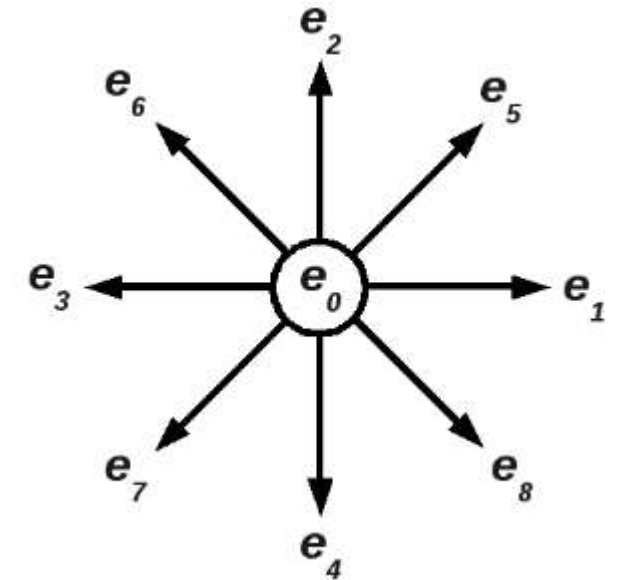


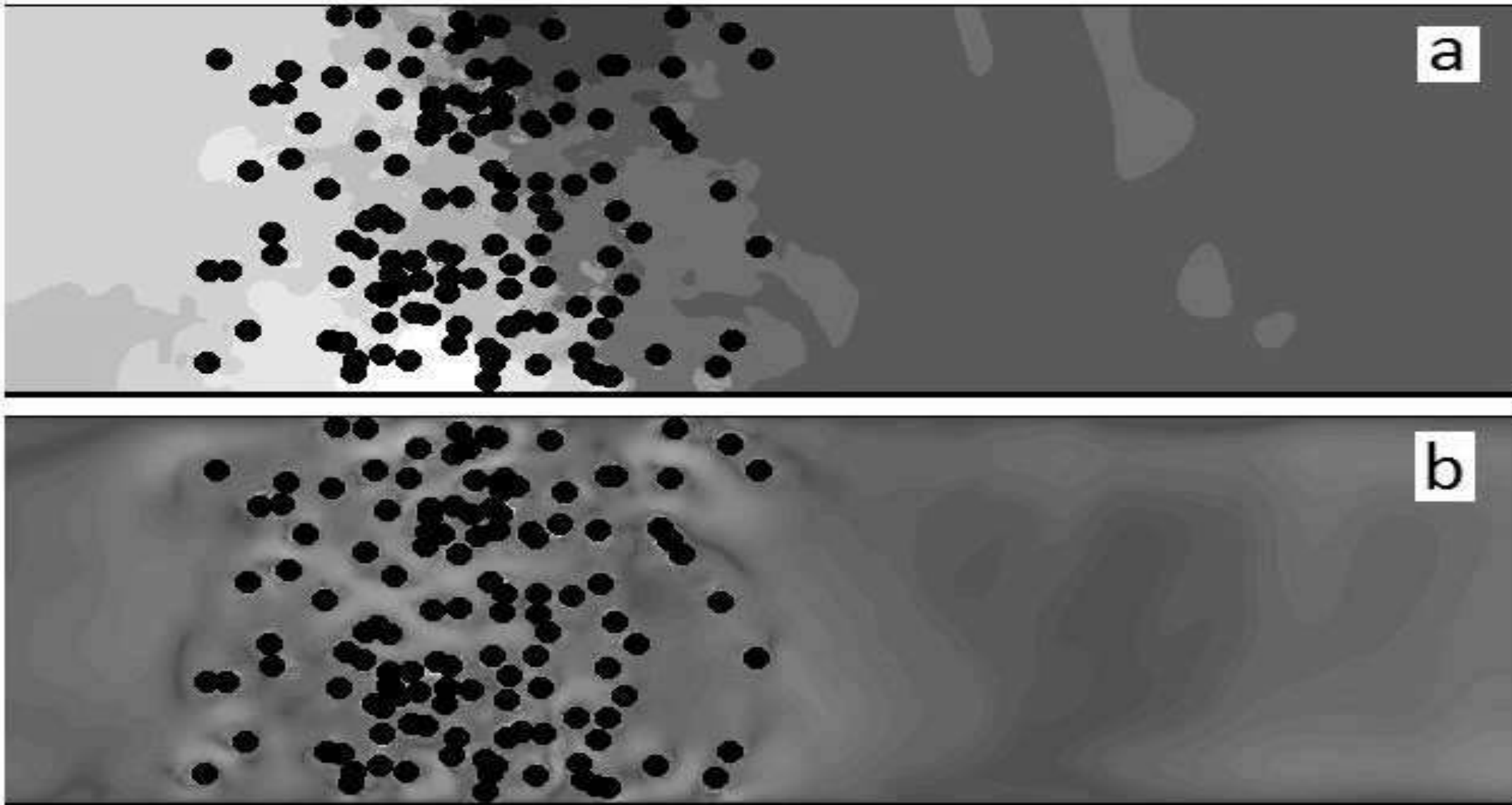
Figure 2

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Figure 3

- Images of iso-pressure (a), and iso-velocity levels.



Values of pressure and velocity corresponds to gray levels from darker (low) to lighter (high).

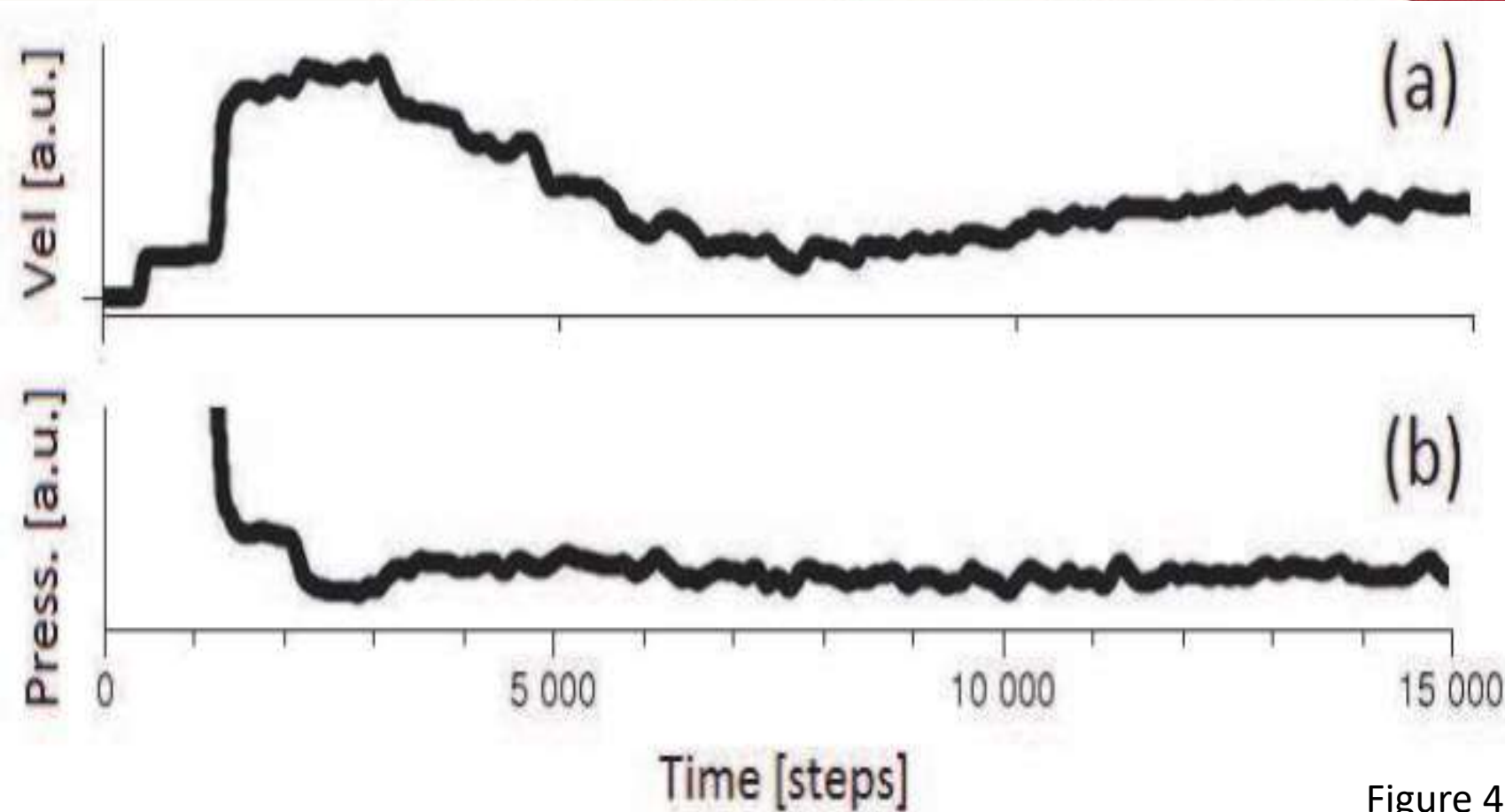
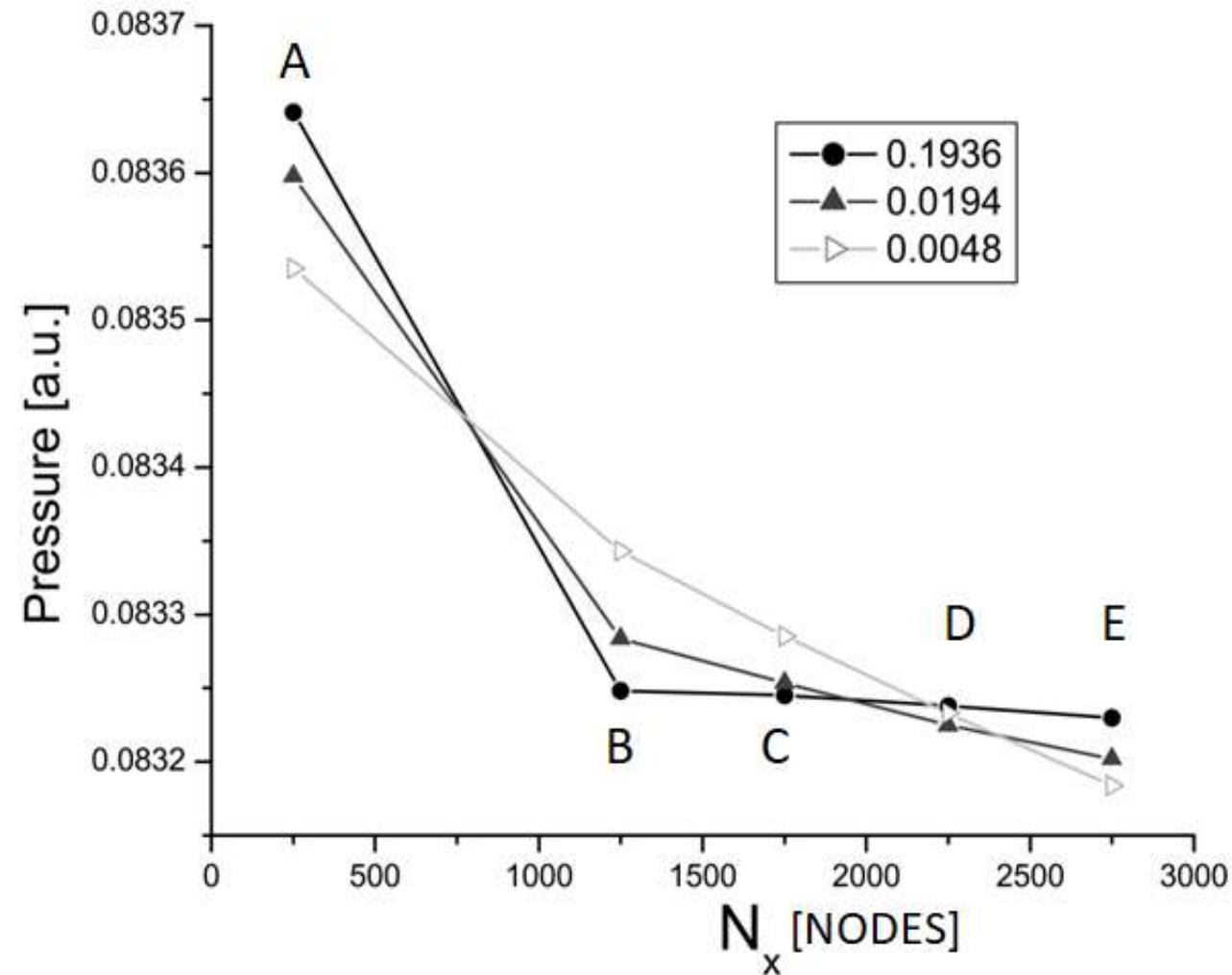


Figure 4

- ▶ Temporal evolution of the velocity (a), and pressure (b) at Point-E in Fig. 1.
- ▶ The high initial pressure variations are due to **initial conditions**.
- ▶ After transients, the pressure is stabilized, only ripples remain due to random disturbance.
- ▶ The long period oscillations of velocity are due to **finite size** of the modeling box.

Figure 5

- Pressure drop measured at points A, B, C, D, and E of figure 1.
- The obstacles strip covers from points A to B; the pressure drop between these two points is about 0.00030 [au]. However out of the strip, the pressure drops only 0.0005 [au].
- Each curve corresponds to a different level of effective area of the obstacle.



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- It was possible to measure the pressure drop (up to 30%) through a dynamic obstacle size (of an averaged 20% of the strip effective-area).

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